

Cancer Detection in Full Field Optical Coherence Tomography Images

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A Multidisciplinary Project

Cancer Diagnosis

rapid tissue analysis

Label-free Imaging

- Full-Field Optical Coherence Tomography (*FFOCT*)
- Dynamic Cell Imaging (*DCI*)



Image Analysis

- exploratory data analysis
- aid-to-diagnosis

Enable use of novel imaging technique for cancer diagnosis via data analysis.

Clinical Context

- **Cancer** – one of the leading cause of death worldwide
- Gold standard for diagnosis is **tissue analysis** / histopathology
- Standard histopathology is **time** consuming, **labor** intensive
- A need for rapid diagnosis in **interventional** settings
- Pathologists **shortage**

Fix

Embed

Slice

Stain

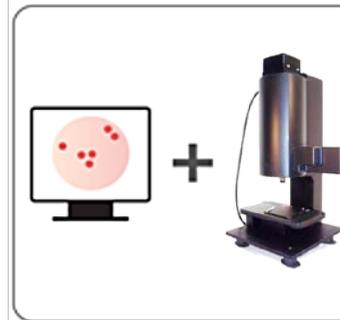
Visualize

Diagnose

Fresh
Tissue

Optical
Slicing

Endogenous
Contrast



novel technique



special training

Gold standard histology



48h



Label-free imaging

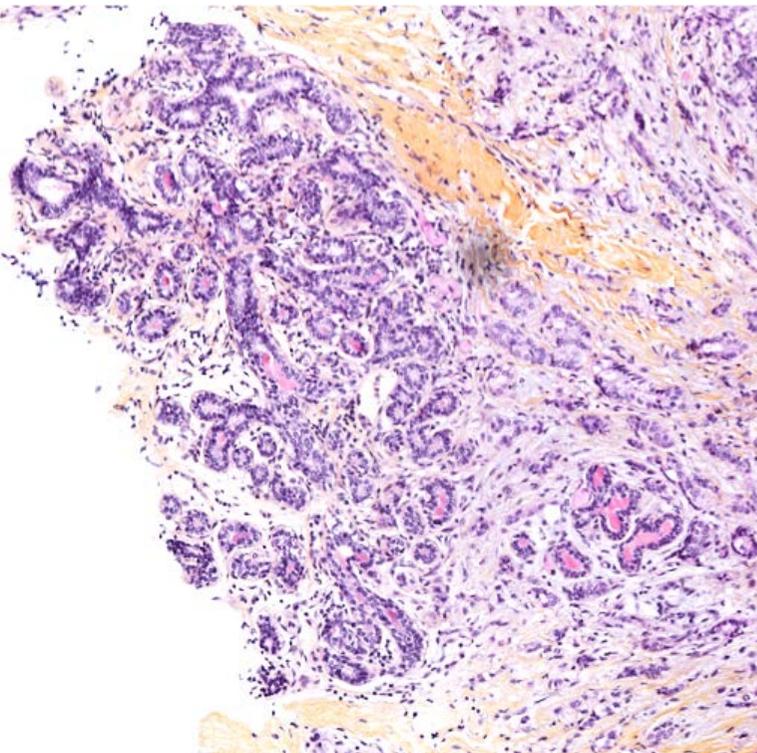


10min

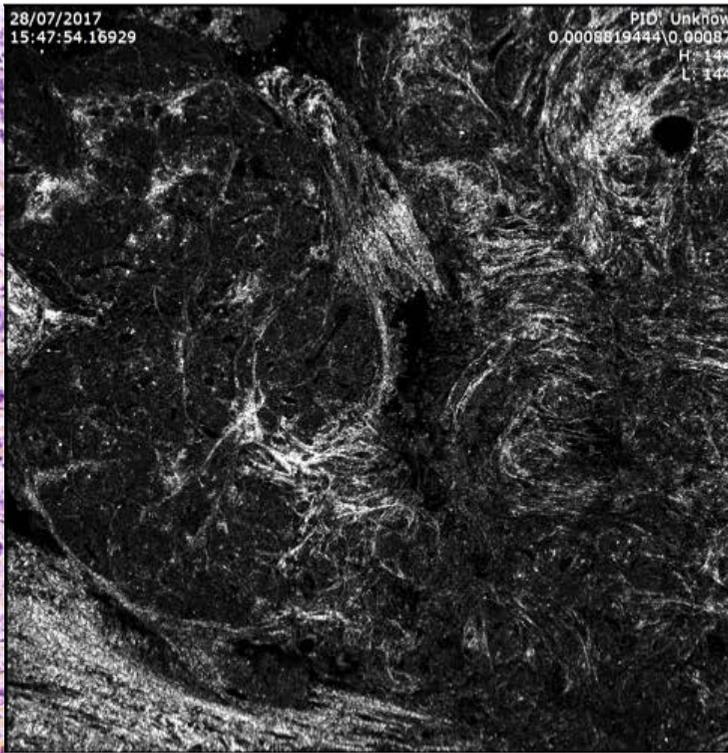
Medical personnel needs training to interpret new contrast.

Imaging Context

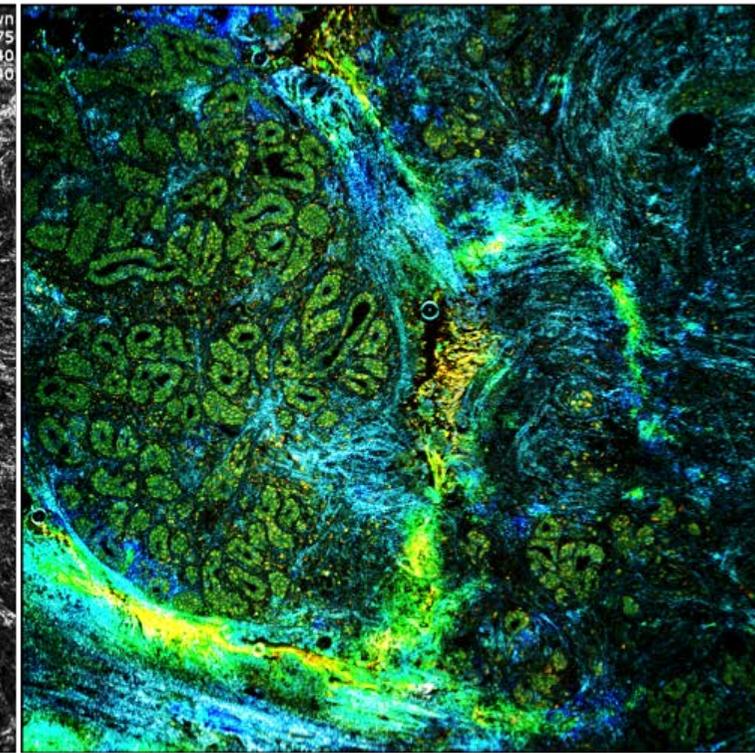
H&E Histology



Full-Field Optical Coherence
Tomography **FFOCT**



Dynamic Cell Imaging **DCI**



normal breast lobule

Full-Field Optical Coherence Tomography **FFOCT**

FFOCT = *en face* OCT

Optical setup : Michelson interferometer

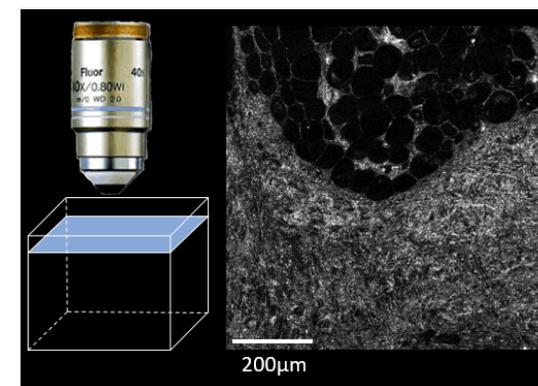
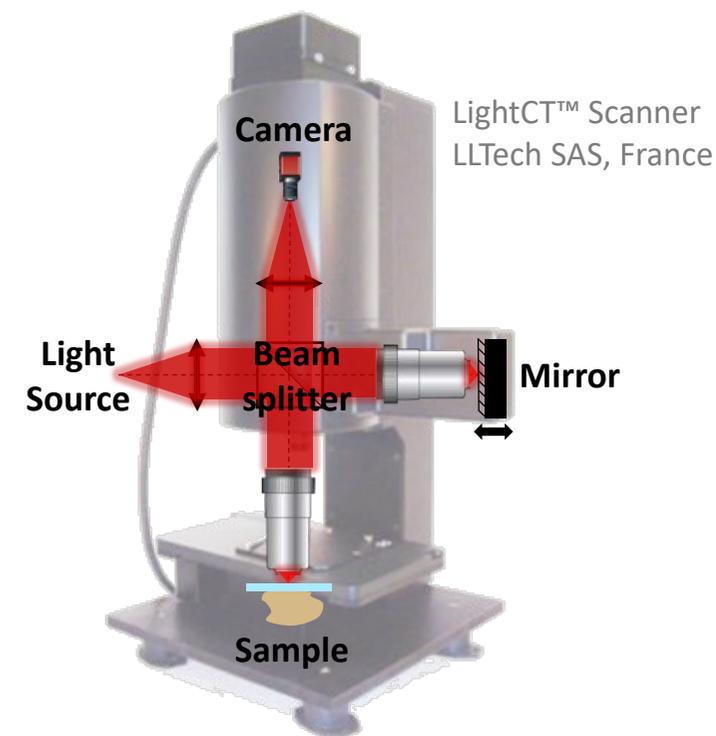
Light interferometry principle :

identical waves amplify when in phase, cancel when not

Low coherence interferometry:

large bandwidth = short coherence length \propto Z resolution

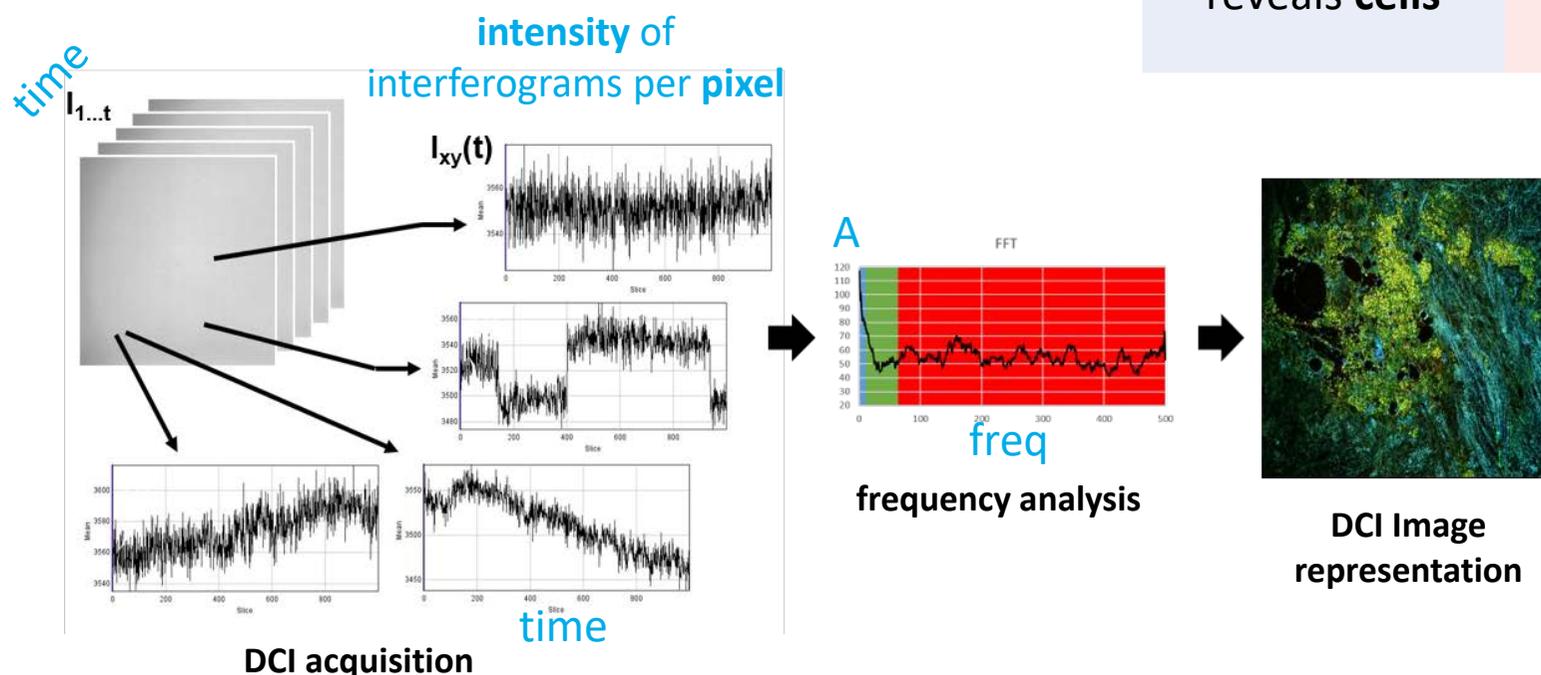
PROS	CONS
good resolution (1 μ m)	no cell information
fast (seconds)	
reveals fibers	



Dynamic Cell Imaging DCI

- overcomes **strong** signal from *fibers* and reveals **active** intra-cellular structures
- captures confined micro-displacements of scatterers
- from *10ms* Brownian to *6s* migration
- origin of signal presumably *glycolysis* → live tissue

PROS	CONS
good resolution (1 μ m)	motion artefacts
fast (minutes)	variable fiber contrast
reveals cells	image representation



Methodology Outline

Can we **extract** more info from DCI **signal** ?

What can we **learn** from DCI **images** ?

Can we learn **fiber representation** in DCI from FFOCT ?

Can DCI be **routinely** used in **clinical** applications ?

Data Exploration

DCI Signal

DCI Images

Multi-modality

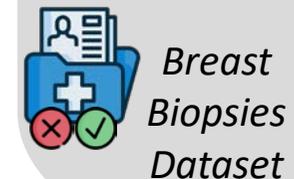
Clinical application

- Source separation

- Fully-supervised classification

- FFOCT/DCI cross-modal representation learning

- Multiple Instance Learning classification



Breast Surgical Excisions Dataset

Goal : feasibility study to discern **pathological** from **healthy** tissue in DCI

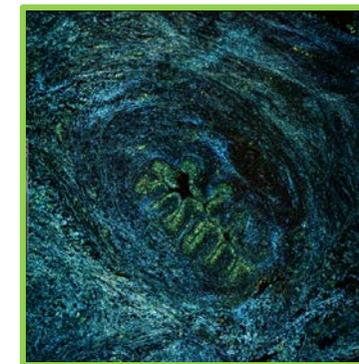
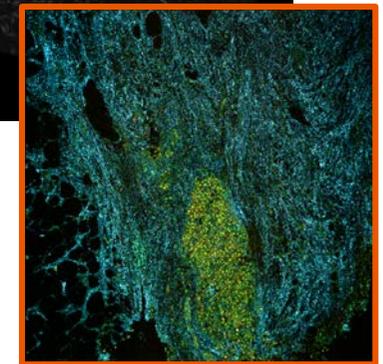
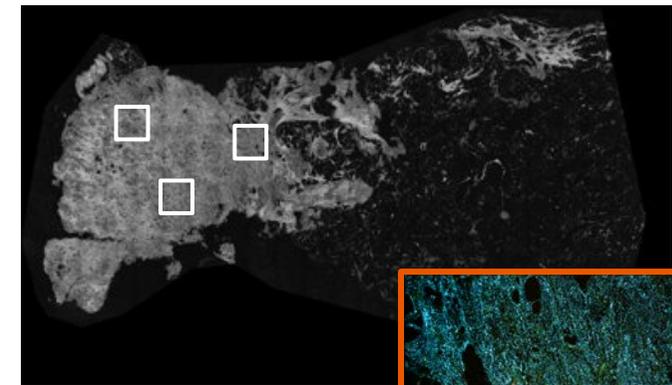
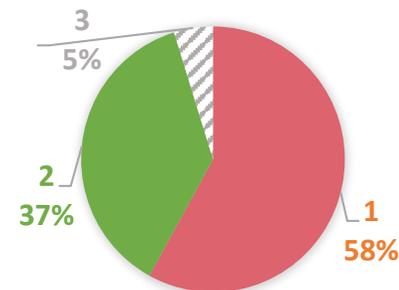
Cohort :

- 33 patients, **mastectomies**
- 47 samples, 11 **healthy** and 36 **tumoral**
- several ROIs per sample ~10 (3 to 16) ROIs / sample

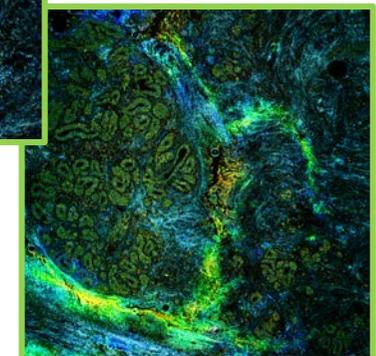
Diagnostic : per ROI with H&E correlations, by pathologist

Dataset :

- ROIs:
 - 279 cancer
 - 179 normal
 - 23 uncertain



1440 x 1440 px



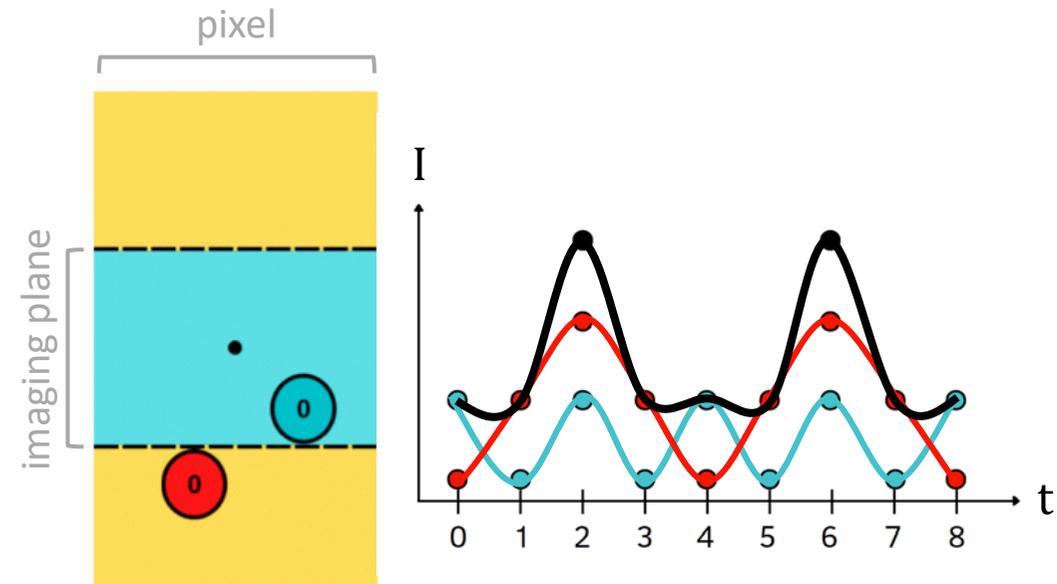
1 Exploring DCI Signal

Hypothesis

- multiple **oscillatory behaviors** present
- **overlapping** scatterers per pixel

Strategy

signal
separation



Two scatterers moving inside a pixel relative to the focal plane & the acquired pixel **intensity**

$$I(t) = I_1(t) + I_2(t)$$

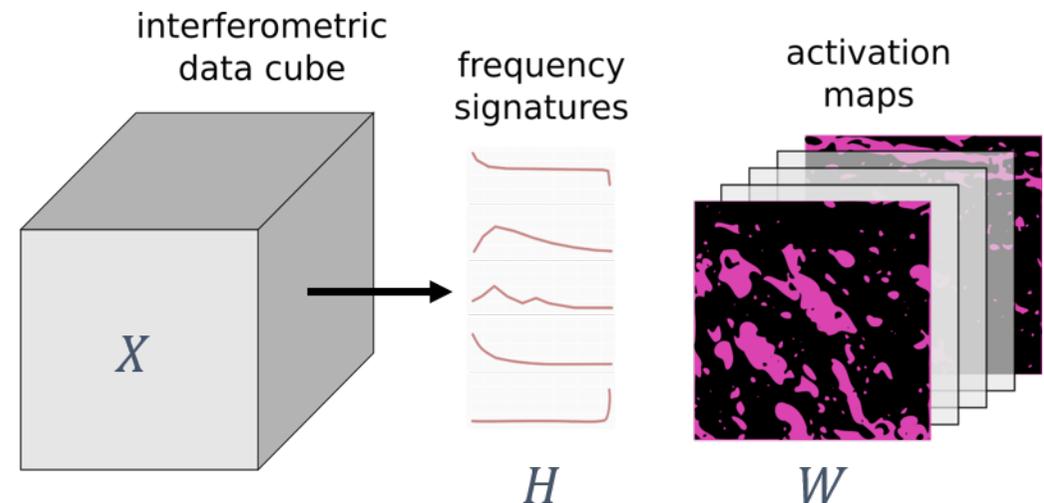
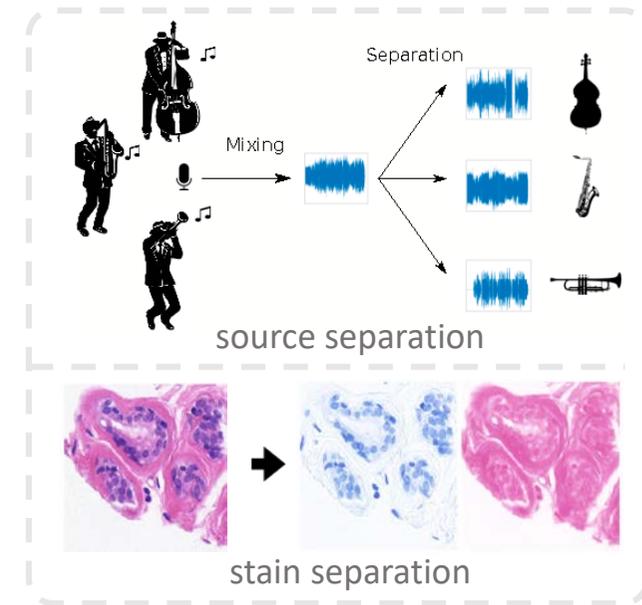
1 Exploring DCI Signal

Signal Separation

- recover the **independent** component signals from a **mixture** signal
- non-negative matrix factorization (**NMF**)

$$\min_{W \in \mathbb{R}^{n \times k}, H \in \mathbb{R}^{k \times f}} \|X - WH\|_F^2 \text{ s.t. } W \geq 0, H \geq 0$$

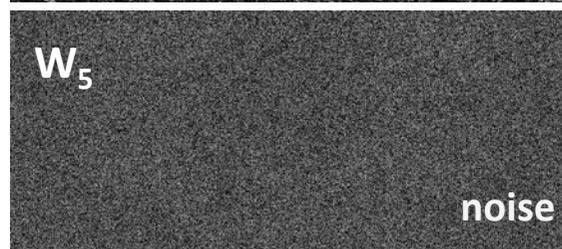
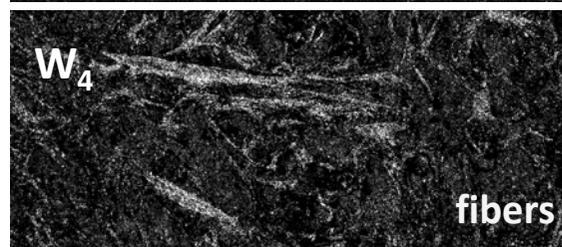
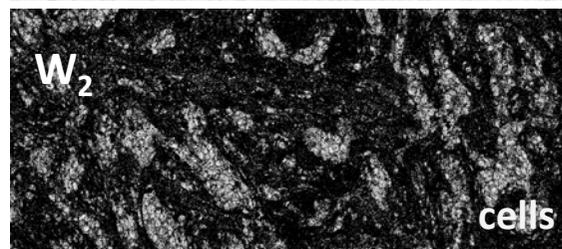
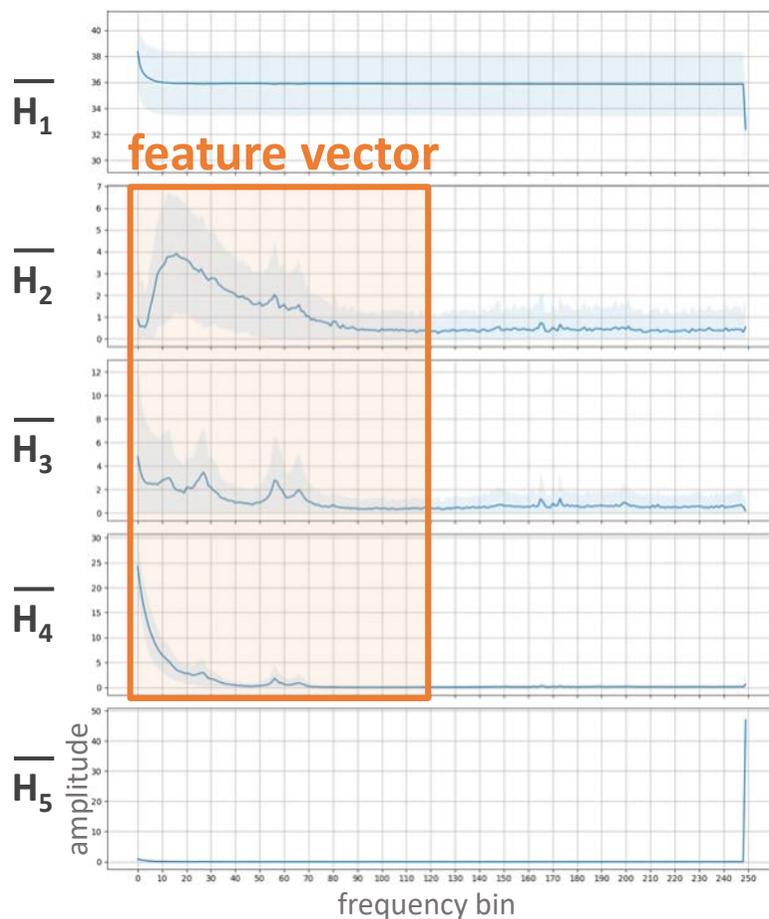
- positive **part-based** decomposition
- **dynamic** and **spatial** components
- empiric choice or rank $k = 5$



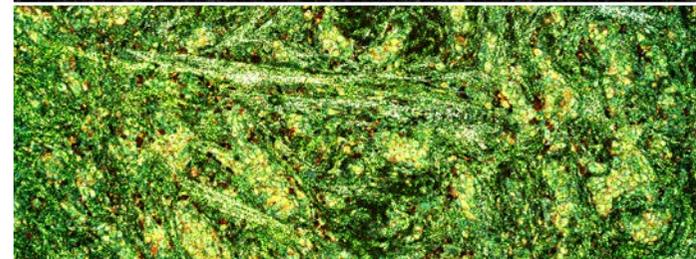
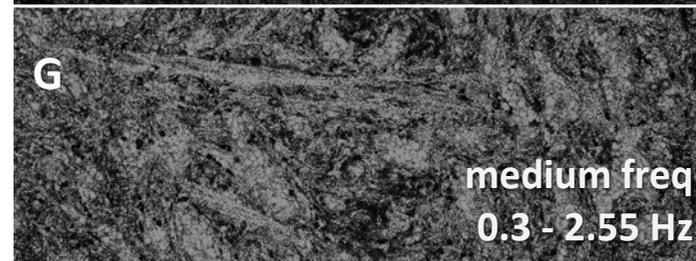
1 Exploring DCI Signal NMF Decomposition Results

$$X \approx WH$$

NMF **dynamic** and **spatial** components



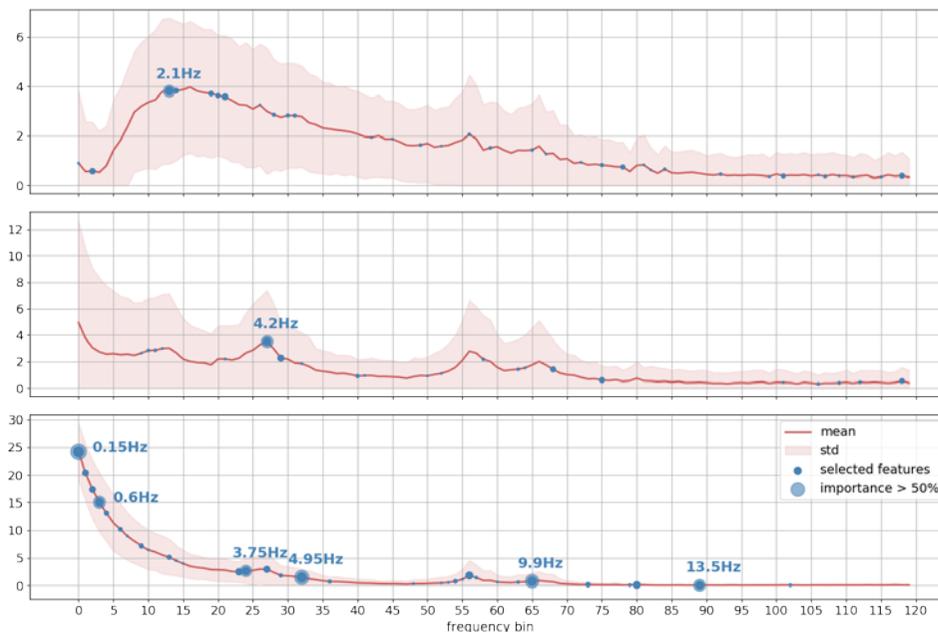
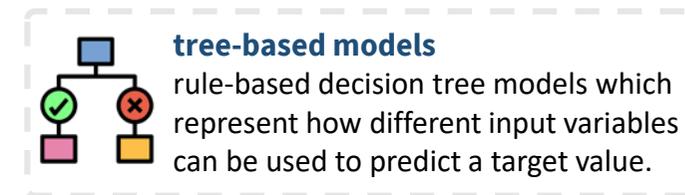
DCI processed image and RGB channels



1 Exploring DCI Signal A Promising Direction

Diagnosis

- train tree-based classifiers (eg. *XGBoost*, *AdaBoost*) on dynamic components only
- normal vs cancer discrimination accuracy $\leq 70\%$
- reveal feature importance



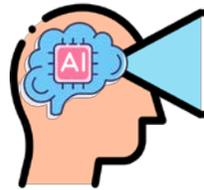
Conclusion

- a **framework** for quantitative analysis of oscillatory behaviors in DCI

What information can be learned from spatial DCI data ?

2 Normal vs Breast Cancer in DCI Images

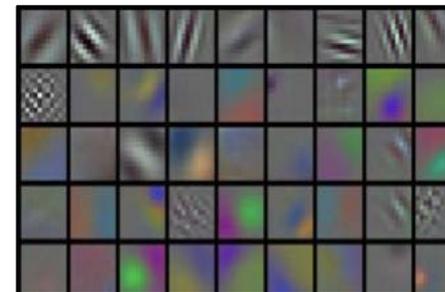
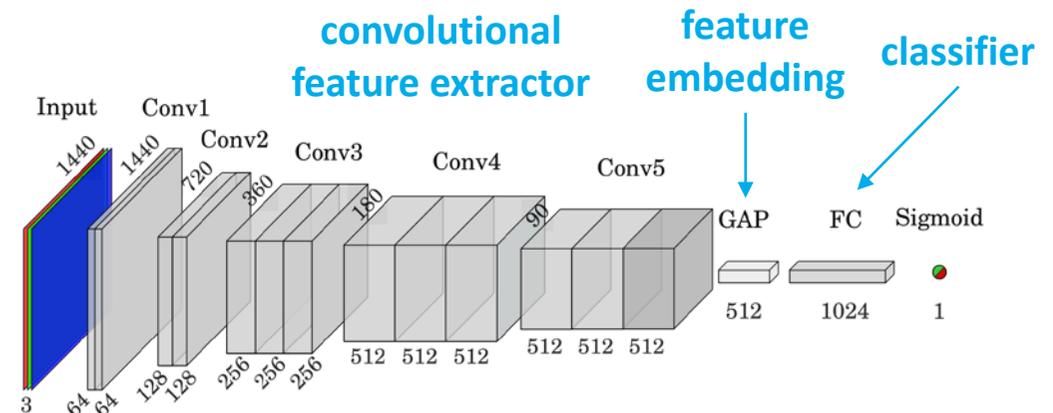
Goal: predict pathologist diagnosis from DCI images.



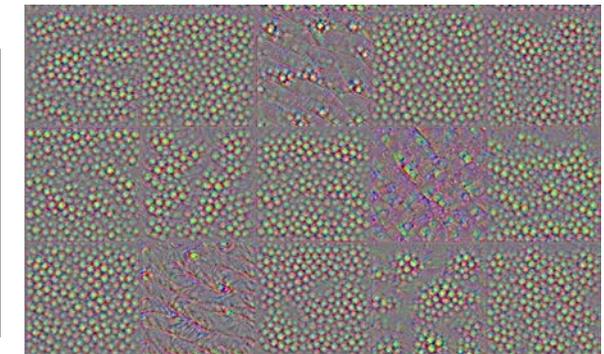
Convolutional Neural Networks (CNN)

ML models inspired by the human vision mechanism

- Learn **patterns** from image examples
- Input image > feature extractor > embedding > classifier > output prediction



low-level features
(e.g. edges, colors)



high-level features
(e.g. cell organization)

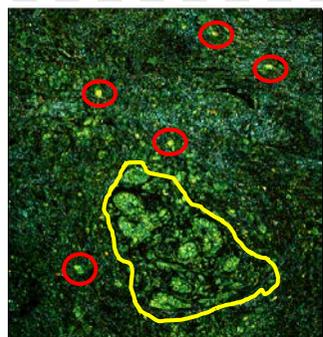
Our Training Strategy:

- ensure **convergence** : limited data → transfer learning, VGG16 / ImageNet
- ensure **generalization** → narrow bottleneck, GAP embedding, dictionary-like

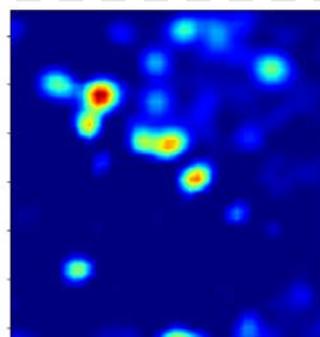
2 An interpretable diagnosis

localization maps - *GradCAM*

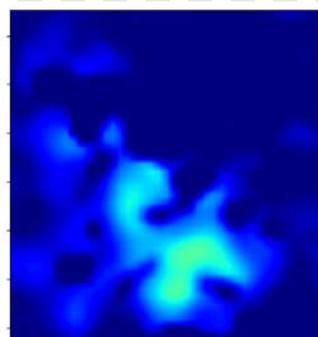
learned patterns - *synthetic input, gradient ascent*



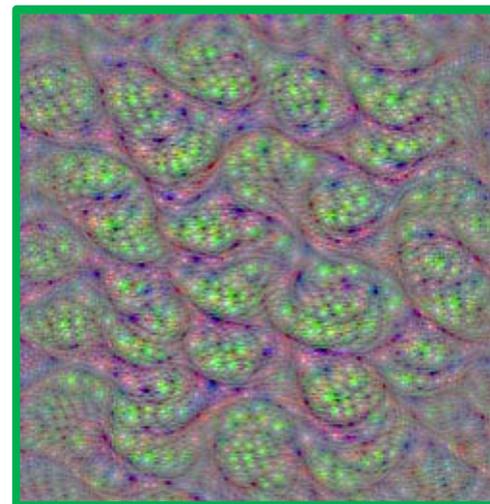
DCI crop of FOV
correctly classified as
tumoral



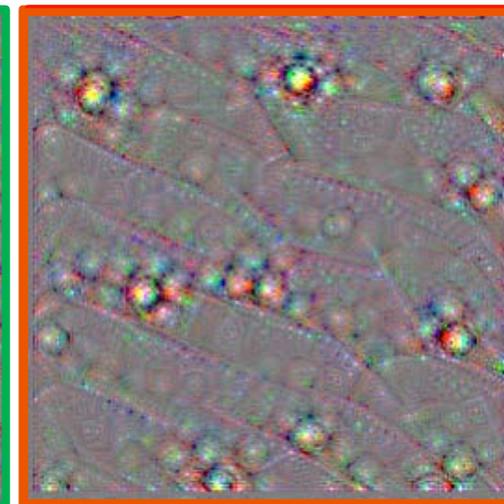
Tumor-positive
localization map
isolated cancer cells



Tumor-negative
localization map
healthy breast lobule

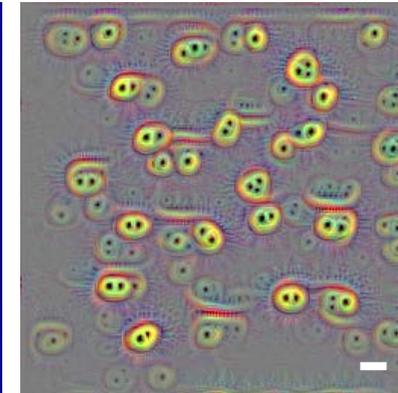
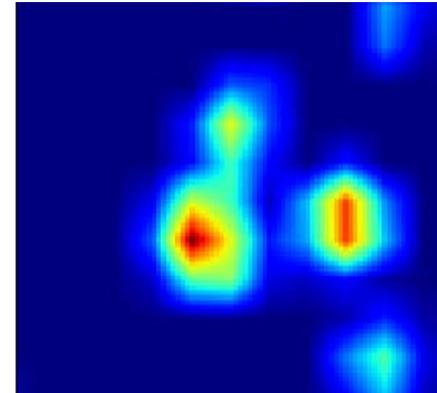
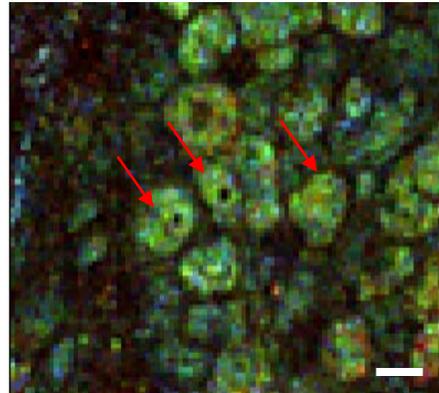
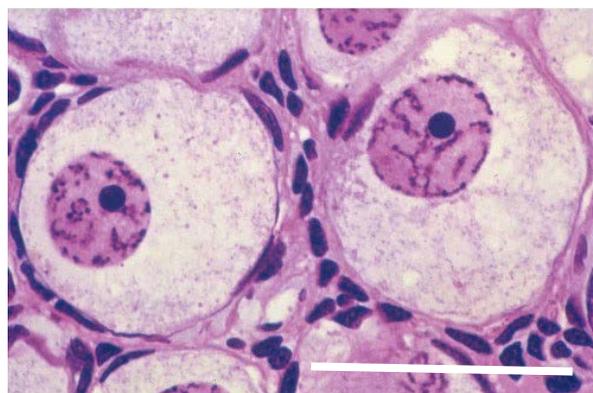


negative evidence



positive evidence

Example of learned *filters* in the last convolutional layer showing different **cell sizes, shapes and organization**, proper to each class



Enlarged **nucleoli** as **biomarker** in DCI: appearance in H&E and DCI, qualitative evidence

2 Fully-supervised Classification Results

Quantitative Results

- Algorithm **surpasses** pathologist performance
 - Possible explanation:
 - ↗ **Sensitivity** : pathologist missed *low contrast isolated* invasive cancer cells
 - ↘ **Specificity** : normal vs in-situ cancer
- Error agreement** between algorithm (3) and pathologists (6)
 - Model *appropriates* **medical reasoning**.
 - Model *overcomes* **human limitations**.
- Performance is robust to adding images with **uncertain** diagnosis
 - Model is *robust* to **ambiguity**.

	Accuracy	Sensitivity	Specificity
pathologist P1	91 %	91 %	92 %
pathologist P2	89 %	94 %	75 %
avg(pathologists)	90 %	93 %	83 %
algorithm ⁽¹⁾	94 %	97 %	85 %

⁽¹⁾ aggregated 5-fold CV test pred

+ 4%

+ 4%

+ 2%

Fully-supervised learning is powerful for diagnosis and cell feature extraction.

3 FFOCT/DCI Cross-Modal Representation

Goal : better characterize **fiber orientation** from DCI

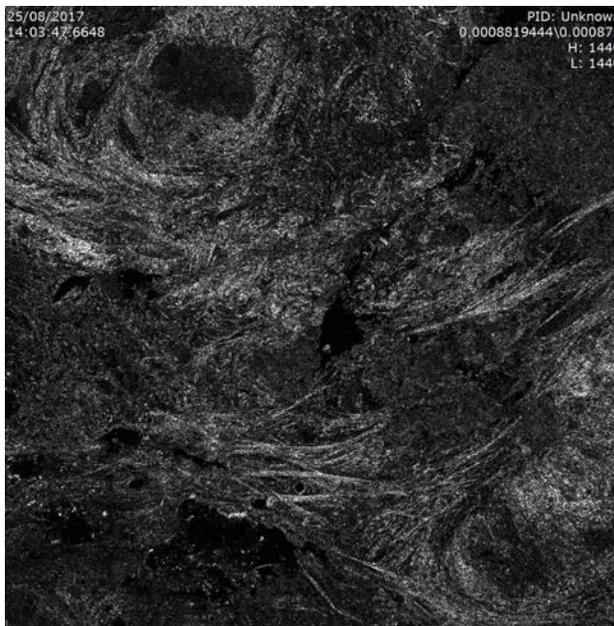
Strategy

- akin to human agent, learn by **contrast** FFOCT / DCI
- train model to **match** corresponding images –
contrastive learning

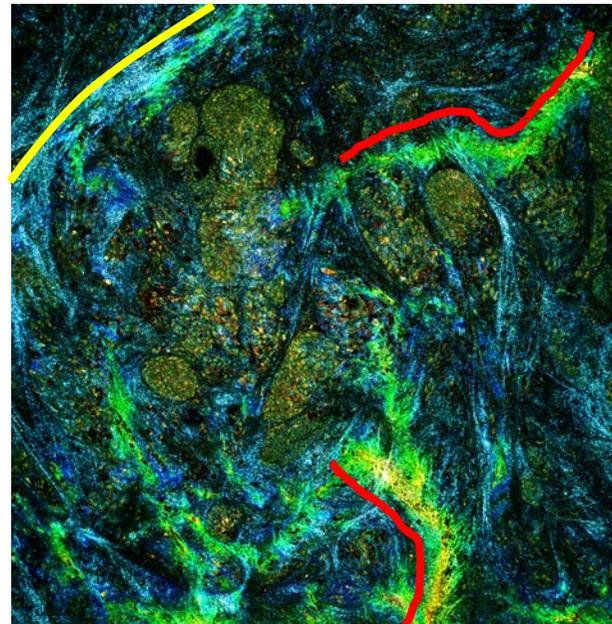


contrastive representation learning

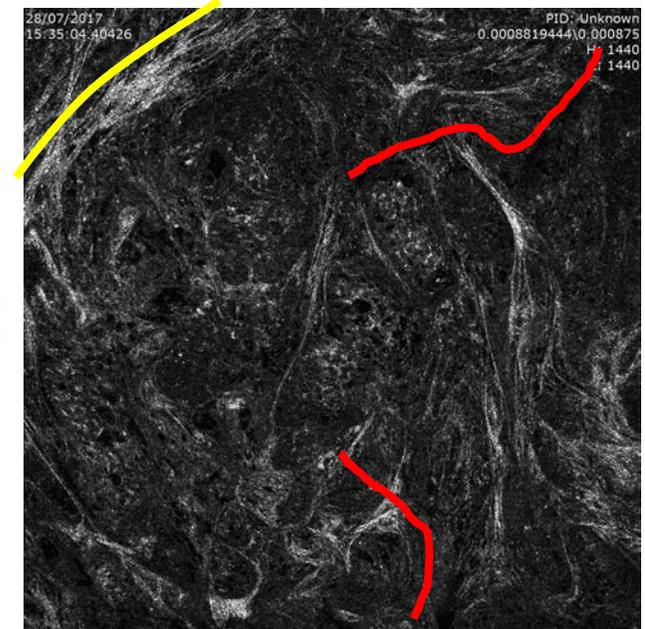
ML paradigm for building an embedding space in which similar sample pairs stay close to each other while dissimilar ones are far apart.



≠

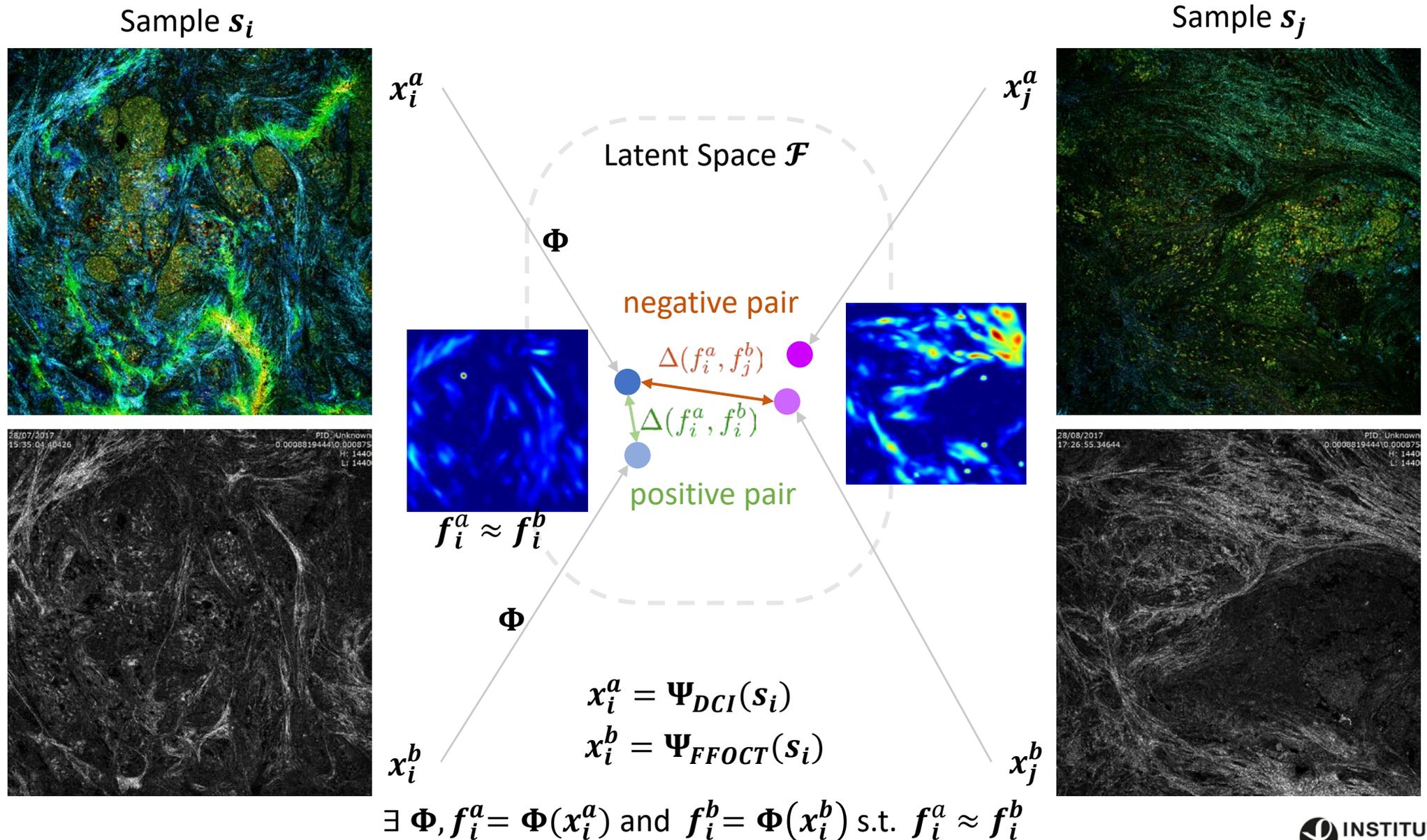


=



Cross-modal matching = pretext task for robust fiber representation in DCI.

3 Concept

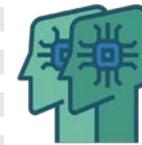


3 Implementation

- Siamese CNN encodes Φ embedding function
- Δ function is **cosine distance** :
 - not sensitive to amount of activation
 - bounded $[0,1]$ \rightarrow binary formulation:

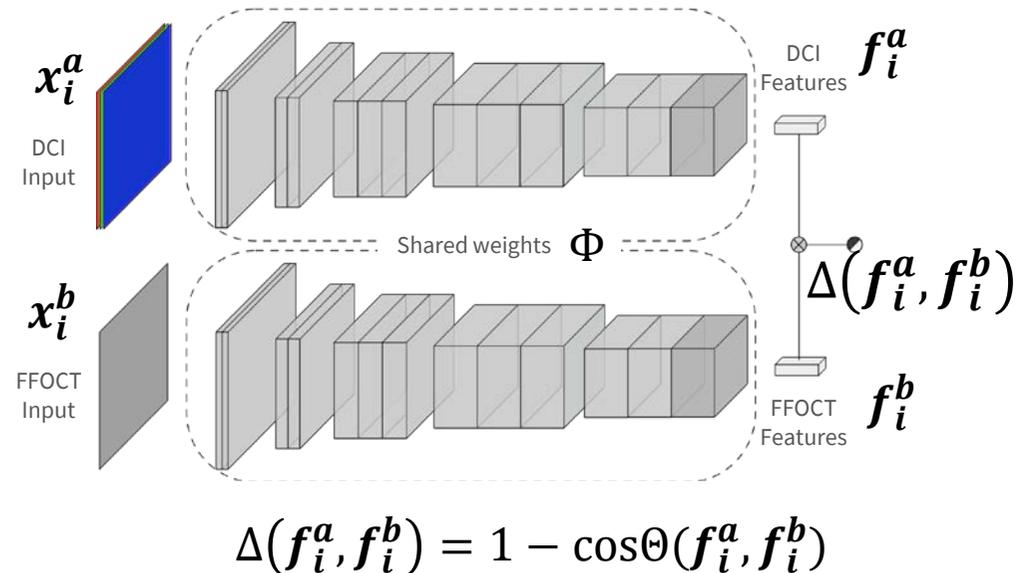
$$L(\theta, \hat{\theta}) = \begin{cases} -\log(\cos(\hat{\theta})) & \text{if } \theta = 0 \\ -\log(1 - \cos(\hat{\theta})) & \text{if } \theta > 0 \end{cases}$$

- “Infinite” dataset generation
 - exploit **registered** images
 - artificially **augment** dataset by extracting corresponding sub-images (480px patches)
 - **online** batch generation (new data every epoch)

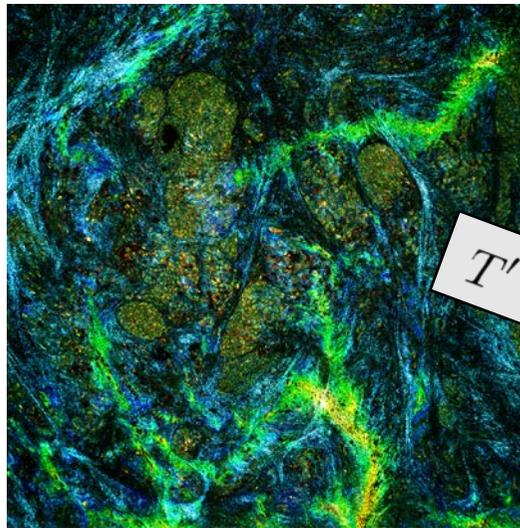
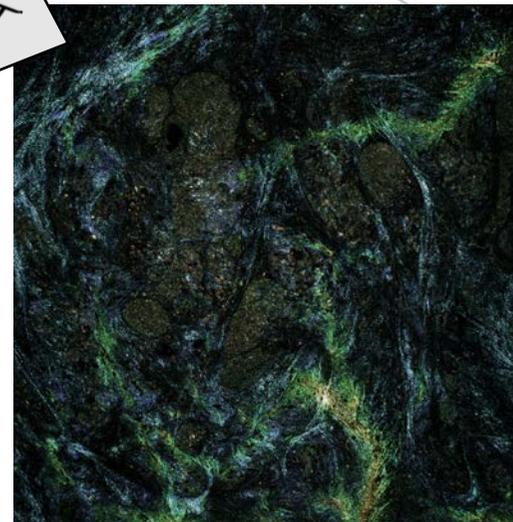
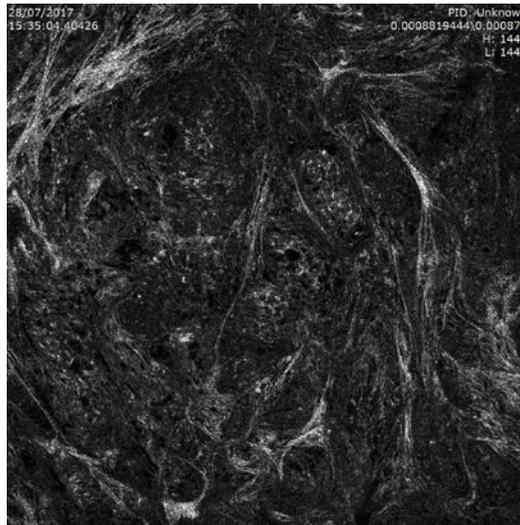


siamese neural network

an artificial neural network containing identical sub-networks working in tandem on different inputs.



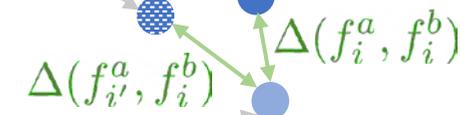
3 Validation Identity Error

Sample s_i  x_i^a  $x_{i'}^a$  x_i^b

$$\varepsilon_{ii'} = \frac{1}{\text{card}(\mathcal{T})} \sum_{i'} |\Delta(f_{i'}^a, f_i^b) - \overline{\Delta(f_{i'}^a, f_i^b)}|$$

where $x_{i'}^a = T'(x_i^a)$ and $T' \in \mathcal{T}$

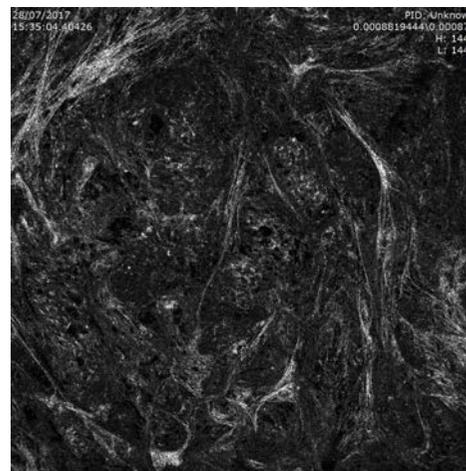
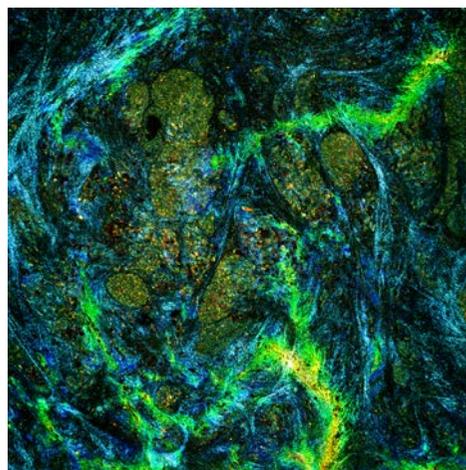
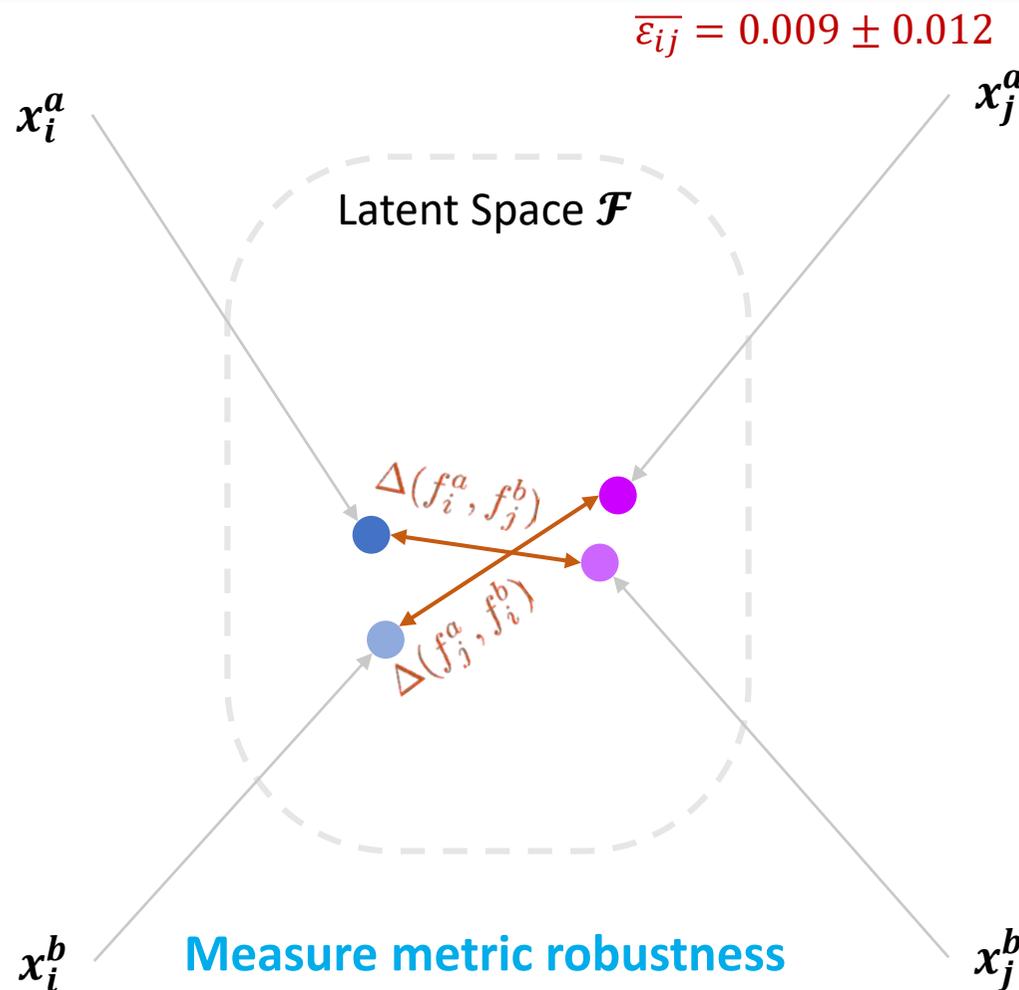
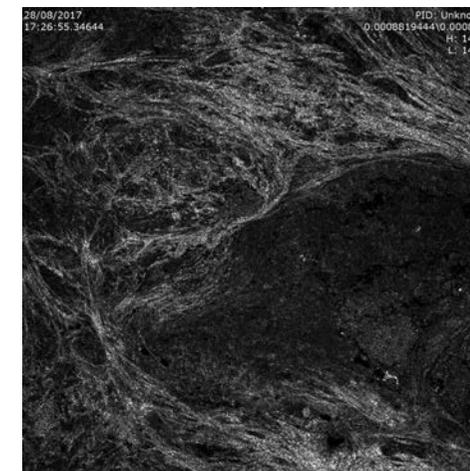
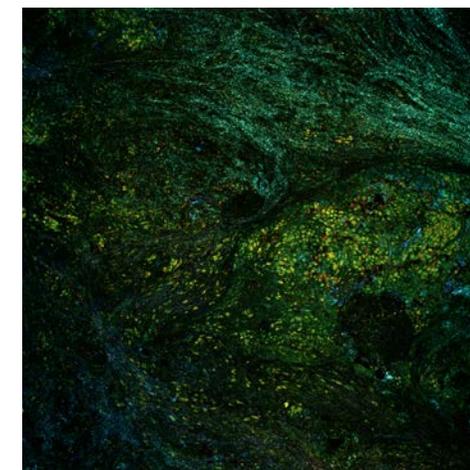
$$\overline{\varepsilon_{ii'}} = 0.004 \pm 0.008$$

Latent Space \mathcal{F} 

Measure metric robustness to slight transforms.

3 Validation Symmetry Error

$$\varepsilon_{ij} = |\Delta(f_i^a, f_j^b) - \Delta(f_j^a, f_i^b)| \text{ where } i \neq j$$

Sample s_i Sample s_j 

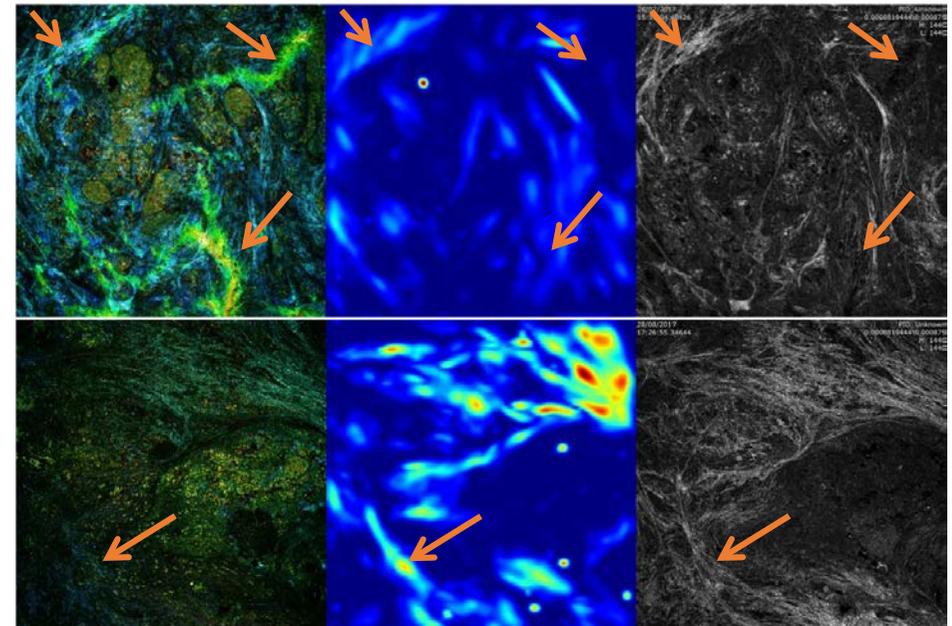
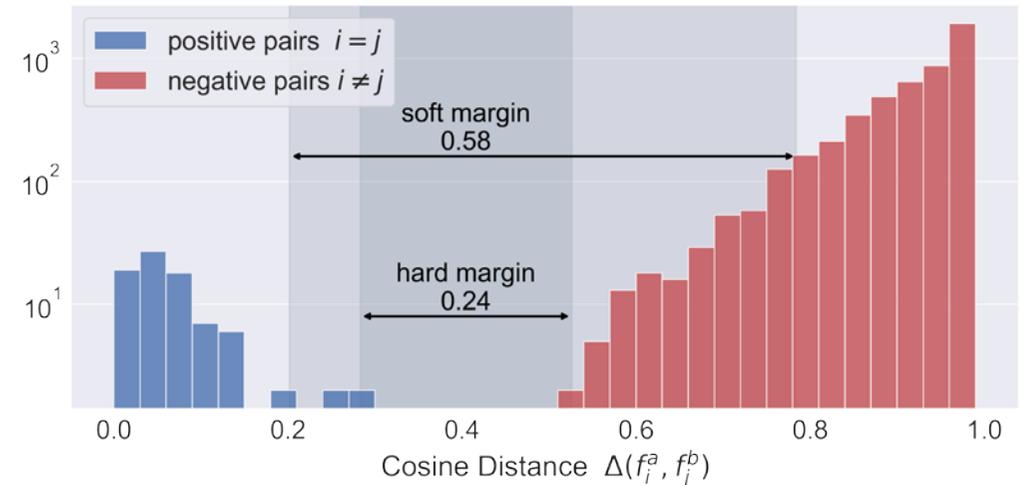
Measure metric robustness to modality choice.

3 Cross-Modal Representation Results

Robust fiber characterization

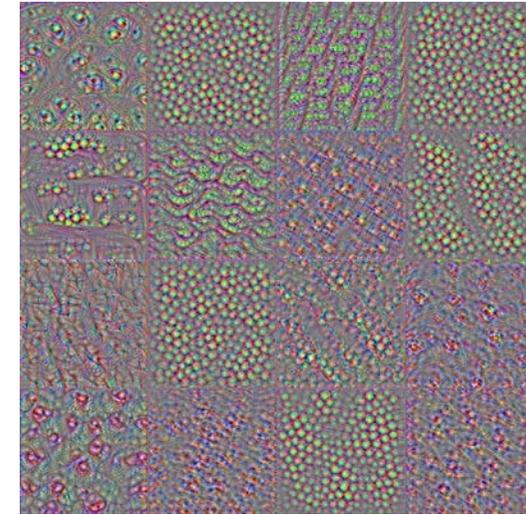
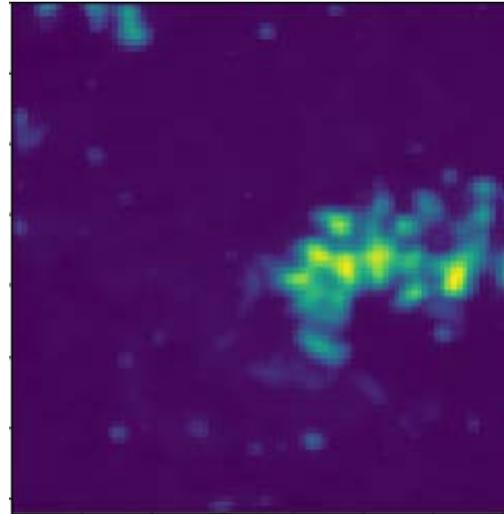
- **Quantitative :**
 - *identity & symmetry errors* <1%
 - implicit **margin** learned
- **Qualitative :**
 - imaging **artifacts** are understood by the network and discounted
 - **low contrast** fibers are captured by the network

Universality : agnostic to dataset → build **general** fiber representation in DCI

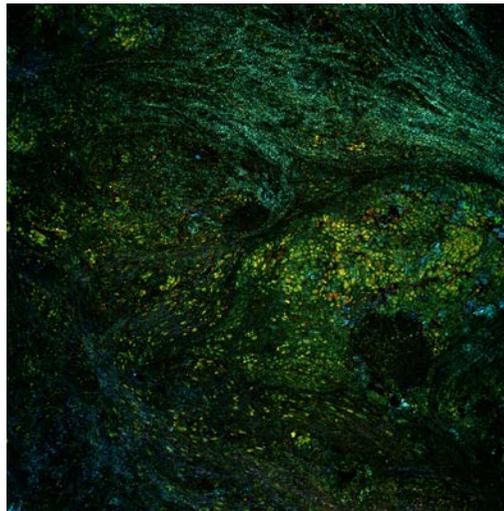


A Complete Characterization of DCI Images

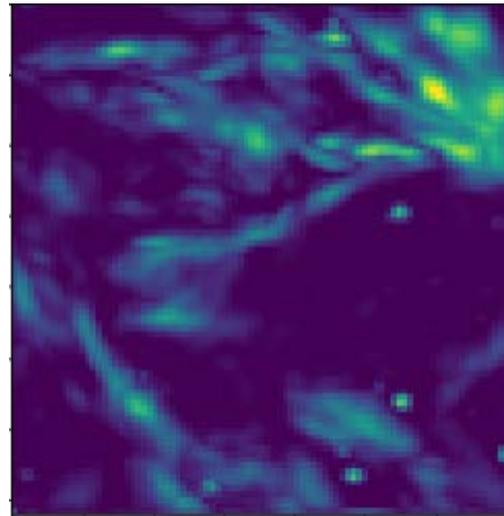
tumor classification model
+
cross-modal matching model
=
full (*cells + fibers*) image **representation**
↓
serve **downstream** tasks
(image coding, signal analysis, diagnosis...)



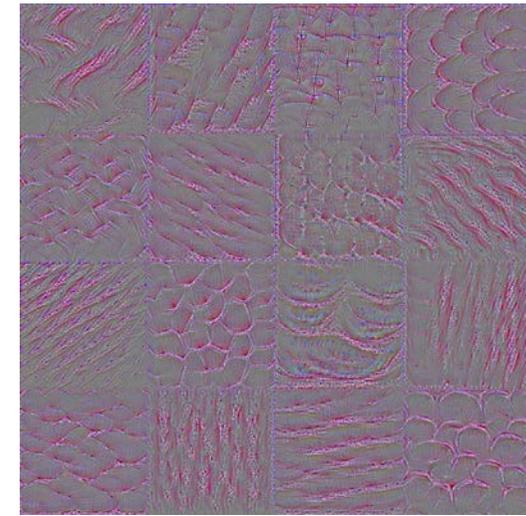
tumor
classification
model
(cell features)



DCI image



localization maps



learned filters

cross-modal
matching
model
(fibers features)

Methodology Outline

Can we **extract** more from DCI **signal** ?

What can we **learn** from DCI **images** ?

Can we learn **fiber representation** in DCI from FFOCT ?

Can DCI be **routinely** used in **clinical** applications ?

Data Exploration

DCI Signal

DCI Images

Multi-modality

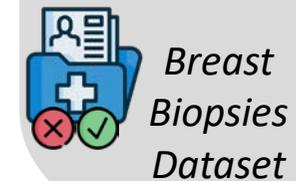
Clinical application

- Source separation

- Fully-supervised classification

- FFOCT/DCI cross-modal representation learning

- Multiple Instance Learning classification



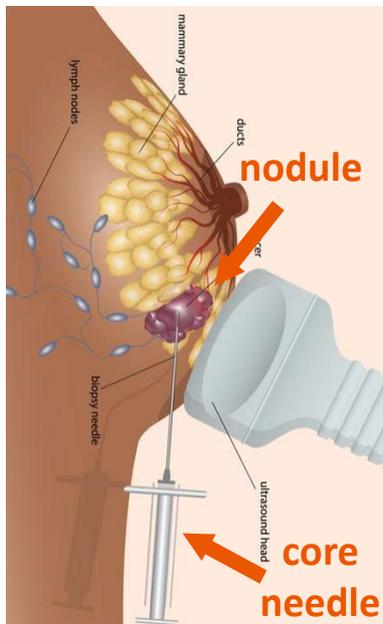
Breast Biopsy Procedure

biopsy = sample tissue from suspect nodule to diagnose malignancy

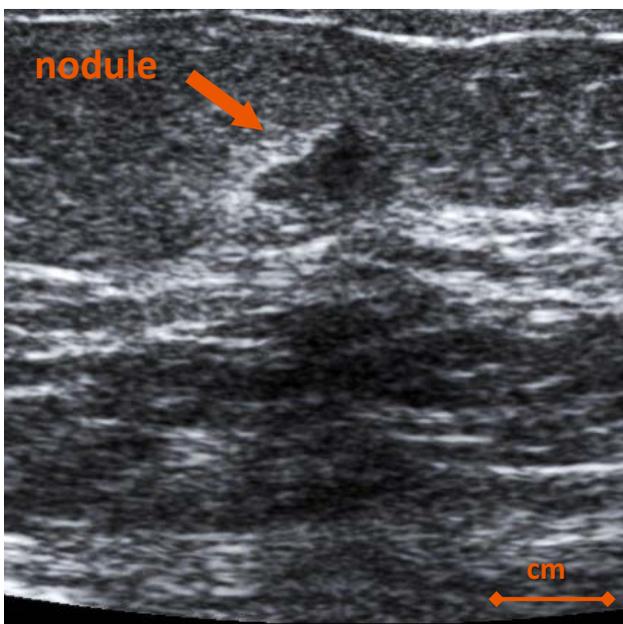
DCI use-cases :

- biopsy **quality assessment** → **minimize** number of biopsies excised
- **rapid** diagnosis → **comfort** patient (80% biopsies not malignant)

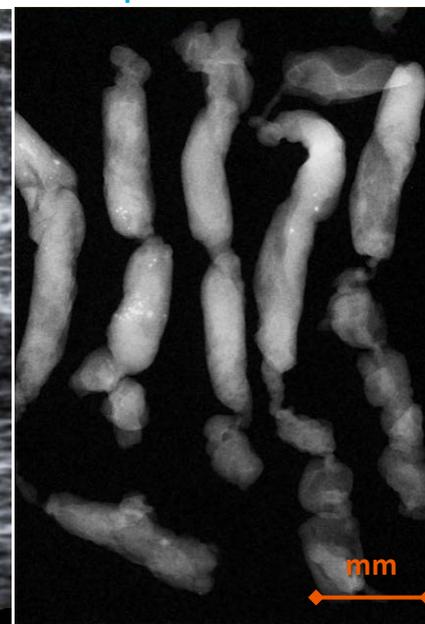
breast biopsy



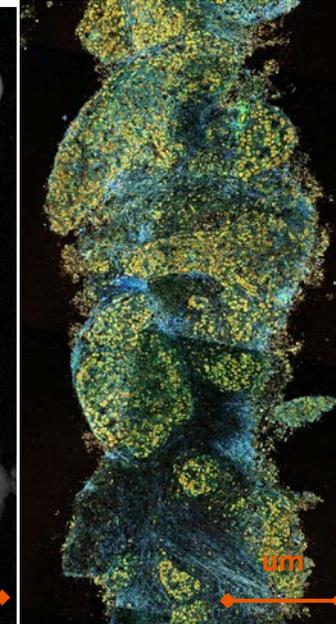
ultrasound guidance



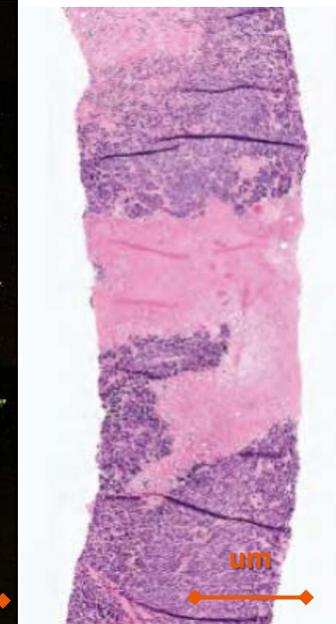
multiple biopsies per nodule



biopsy in DCI



biopsy in H&E histology



minutes



days

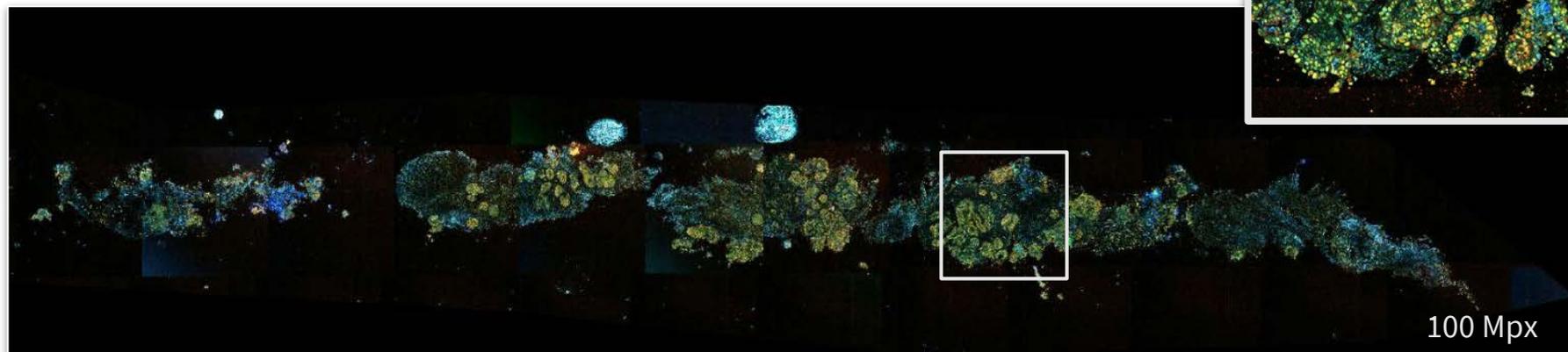
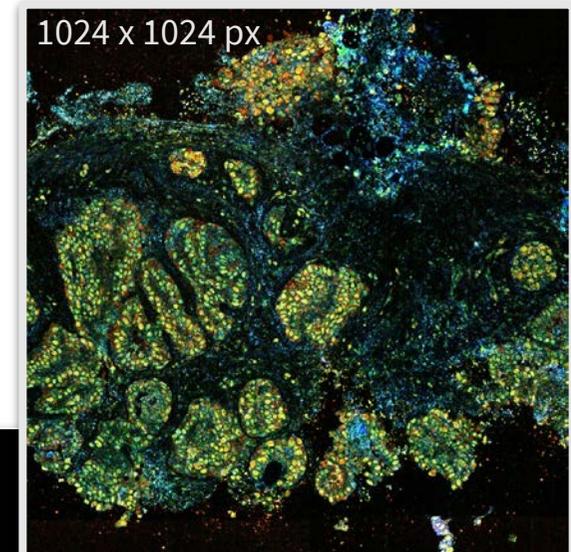
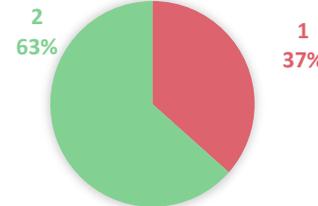
Breast Biopsies Dataset

Cohort : 71 breast nodules

Diagnostic : a histopathology report per nodule, based on H&E

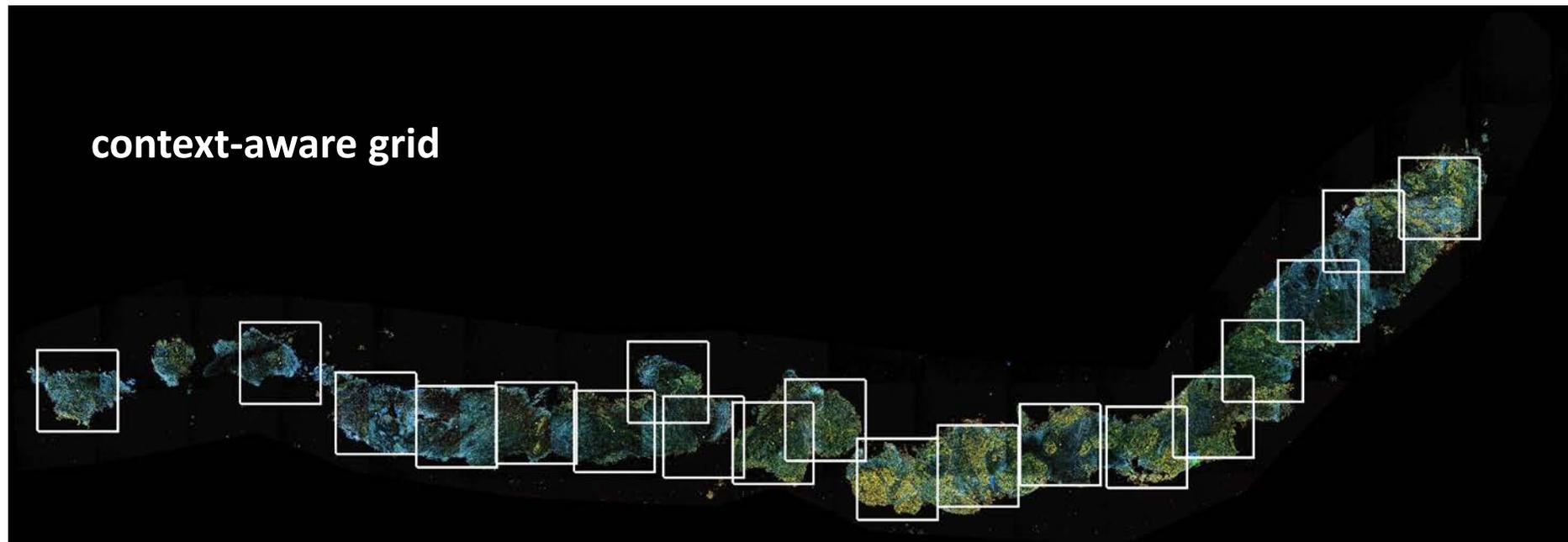
Dataset :

- 71 breast nodules + pathology reports
 - 27 malignant
 - 44 benign
- 145 biopsies in DCI
 - 53 from malignant
 - 92 from benign

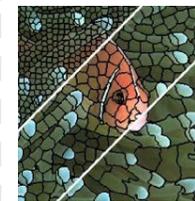


100 Mpx

Breast Biopsies Dataset Image Sampling



- sub-sample image optimally :
 - minimal **fragmentation**
 - avoid splitting **homogenous** structures
 - *SoSleek* - context-aware sampling with SLIC superpixel segmentation
- ⇒ 2K patches of 1024 x 1024 px / 145 biopsies

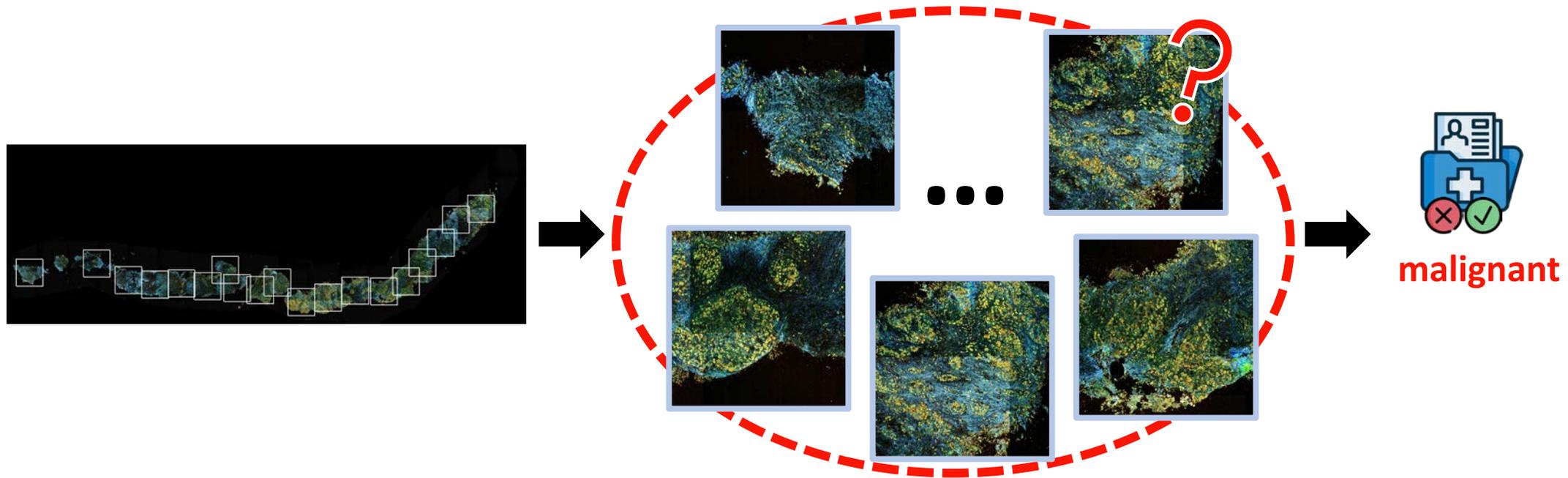


Simple Linear Iterative Clustering (SLIC)
image segmentation method that groups pixels according to their spatial and color proximity.



Sample Optimally with SLIC (SoSleek)
Python package for optimally sampling big images with texture awareness, based on SLIC superpixels.
github.com/dmandache/sleek-patch

Cancer Detection *via* Multiple Instance Learning



one diagnostic per **group** of patches → MIL training paradigm

MIL Assumptions:

- A malignant biopsy contains at least **one** malignant instance.
- A benign biopsy does not contain **any** malignant instances.



Multiple Instance Learning (MIL)

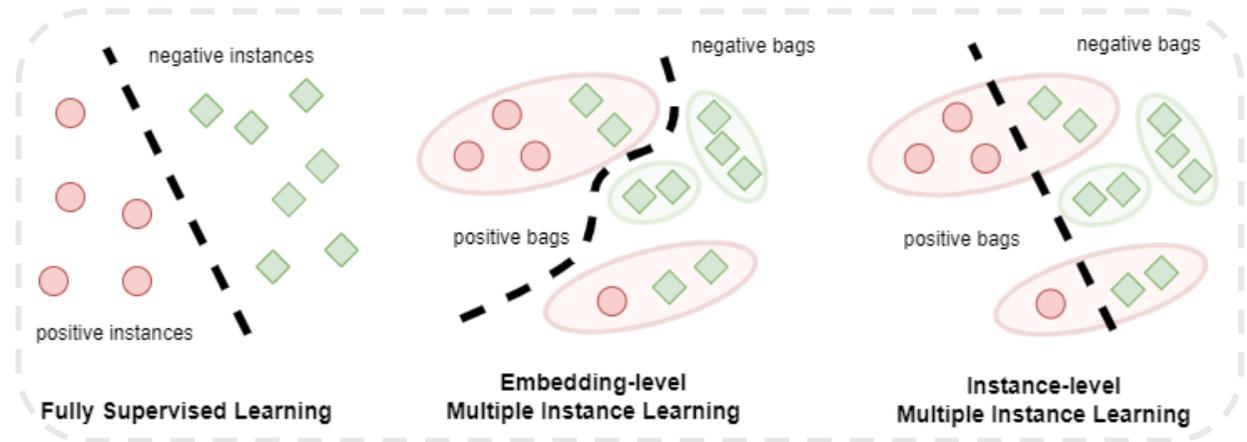
supervised method for learning from labeled groups (bags) of instances and the individual labels are unknown.

Goal: predict **global** (biopsies) and **local** (patches) diagnosis

Multiple Instance Learning

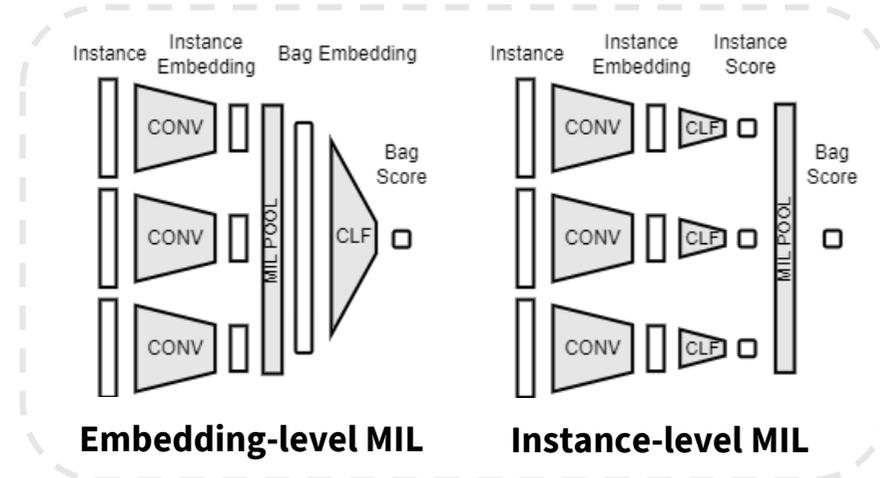
MIL formulations

- Embedding-level MIL
 - global embedding
- Instance-level MIL
 - local scores



Implementation = multi-branch CNN

- computationally heavy
- cannot train end-to-end
- transfer weights (not task-specific)

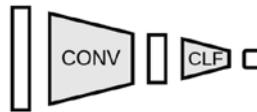


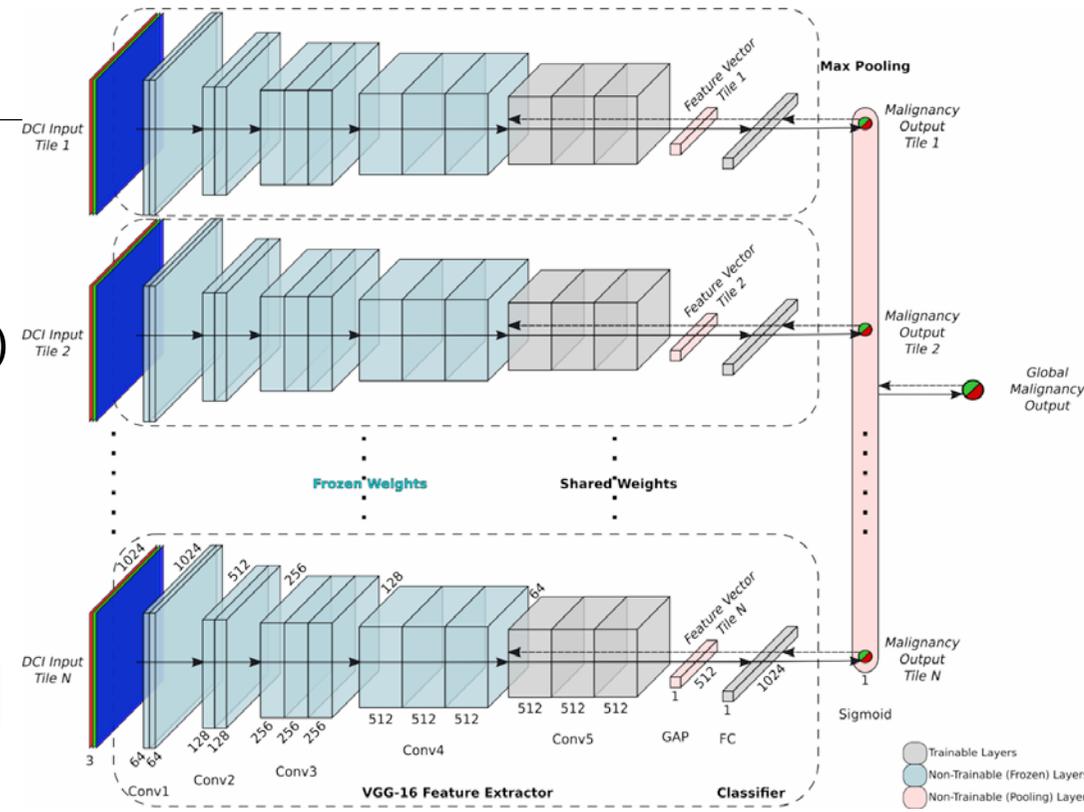
Most MIL applications are embedding-level with transferred feature extractors.

Favor interpretability and task-specific knowledge encoding in MIL.

Implementation

Architecture

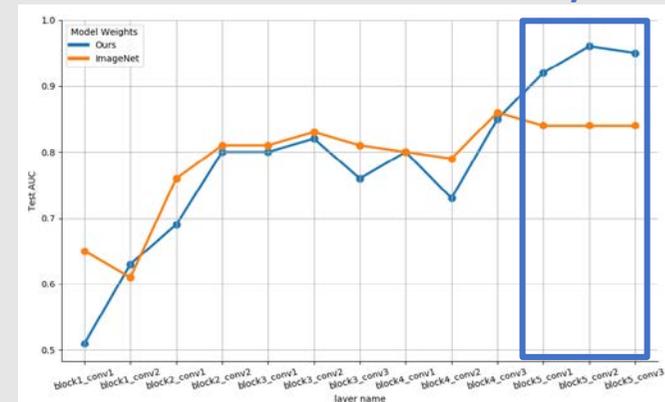
- instance-level MIL with max aggregation implements MIL assumptions $\hat{Y} = \max_i(\hat{y}_i)$
- main branch transferred** from our prior diagnostic task 
- freeze domain specific** feature extractors
- fine-tune task specialized** feature extractors + classifier



Training

- $\mathcal{L}(\hat{Y}, Y) = \mathcal{L}(\max_i(\hat{y}_i), Y)$
- Focal Loss
 - focus on hard examples $FL = -(1 - P)^{\gamma} \log(P)$
 - 8%** accuracy gain vs CE $CE = -\log(P)$

Which layers to freeze? **task-specialized layers**

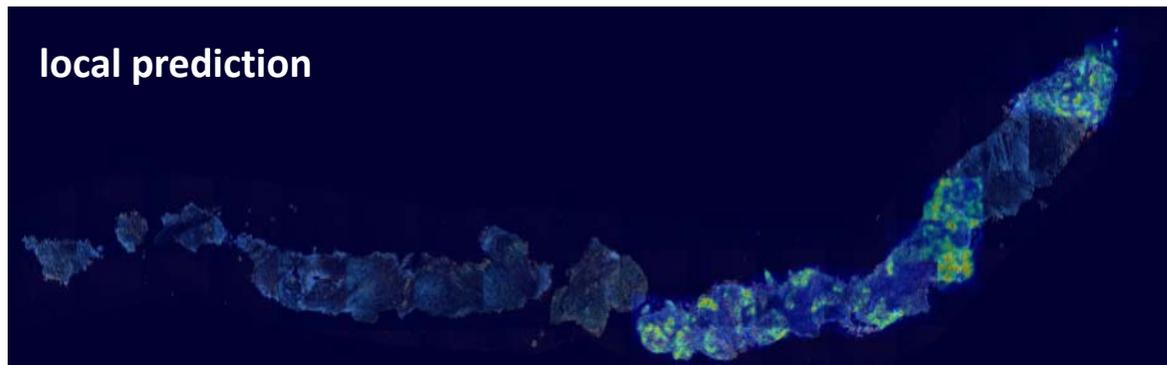


Results

- intra-domain pre-training allows **convergence**
- relevant metric assessment:

Not all biopsies of same nodule might be malignant.

- specificity at **biopsy** level **90 %**
- sensitivity at **nodule** level **89 %**
- **clinical acceptability criteria:**
 - specificity > **90%**
 - sensitivity > **80%**
- improve with local ground truth *OR* embedding-level MIL



Intra-domain vs Extra-domain pre-training

	Datasets	Test Metrics		
		Accuracy	Sensitivity	Specificity
Intra	ImageNet + BiopsyData	72 %	57 %	82 %
	SurgeryData + BiopsyData	86 %	89 %	84 %
Extra		+ 14 %	+ 32 %	+ 2 %

	Test Metrics		
	Accuracy	Sensitivity	Specificity
biopsy	85 %	76 %	90 %
nodule	86 %	89 %	84 %

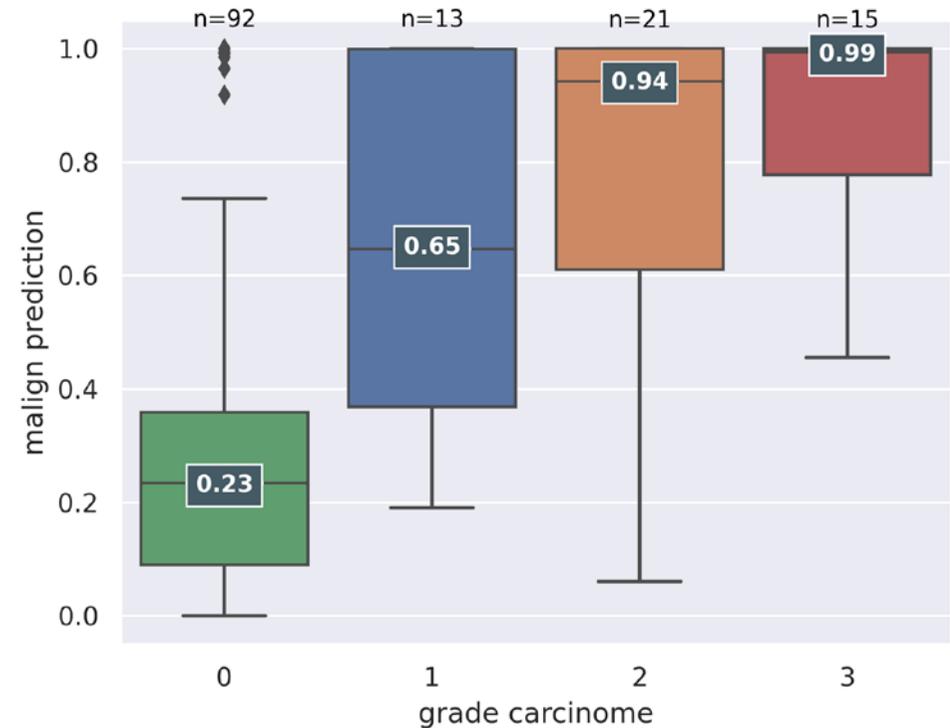
Prediction Analysis

Benign tumors and high grade cancers have more chance to be identified.

Malignancy Grade	True Prediction
1	70 %
2	76 %
3	87 %
1+2+3	75 %
0	90 %

 **emergency intervention**
 **screening**

prediction accuracy according to malignancy grade

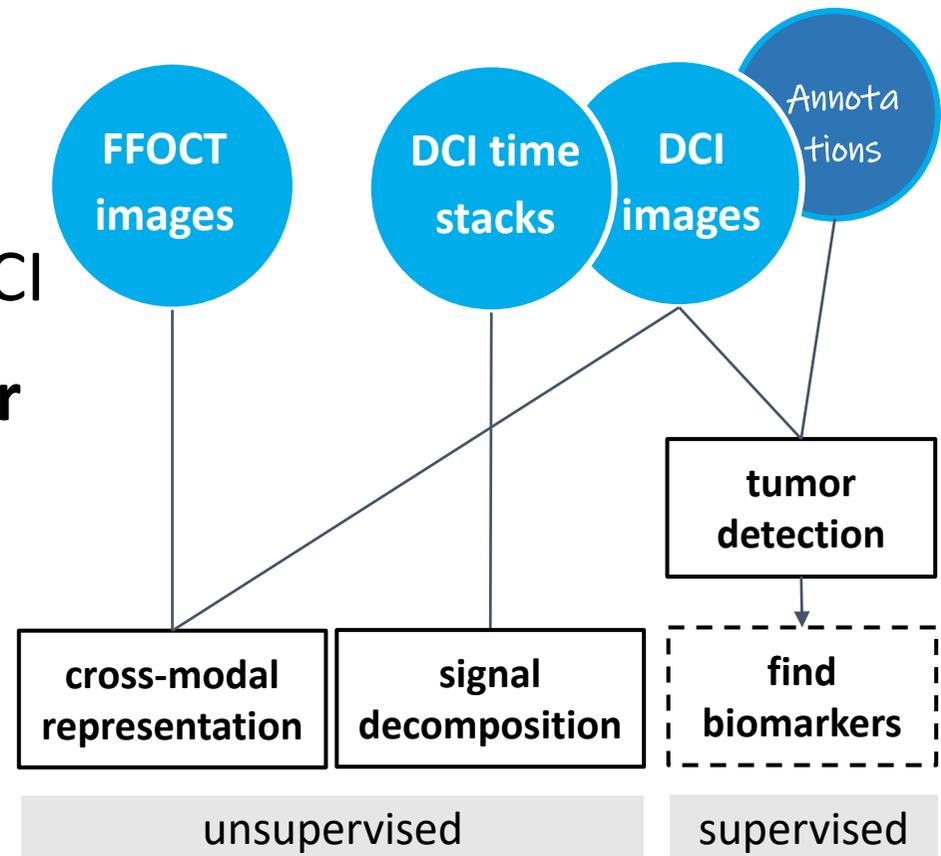


sample prediction according to malignancy grade

Find best use-case for DCI: screening, emergency intervention.

Conclusions Data Exploration

- ✓ framework for extracting **oscillatory signatures**
- ✓ *robust fiber characterization* in DCI
- ✓ *interpretable CNN tumor classifier* which *surpasses* pathologist performance
- ✓ *evidence* towards considering enlarged **nucleoli** as cancer **biomarker** in DCI



Better characterization of DCI data.

Conclusions Clinical Application

diagnosis method for real-world **clinical** application :

- ✓ *remove* expert **annotation** bottleneck
- ✓ *predict* **local** diagnosis without explicit training
→ interpretability
- ✓ *facilitate* **datasets** and **aid-to-diagnosis model** development

Efficient aid-to-diagnosis model development without disturbing clinical protocol.

Speed-up the adoption of DCI.

Perspectives

- ❑ **dynamic** signal analysis + cell/fiber **localization maps** as ground truth
 - supervised source separation
- ❑ include corresponding **histology images**
 - preparation protocol correlated with DCI acquisition
 - multi-modal contrastive learning
- ❑ **metabolic** analysis + dynamic signal analysis
 - 10x glycolysis rate in cancer cells (Warburg effect)

Efforts towards better image representation and biological understanding.

Thank you ! **Merci !** Mulțumesc !

INSTITUT PASTEUR
Bioimage Analysis Unit

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Institut Pasteur
Vannary Meas-Yedid
Jean-Christophe Olivo-Marin
♥ all BIA members 2017-2022 ♥
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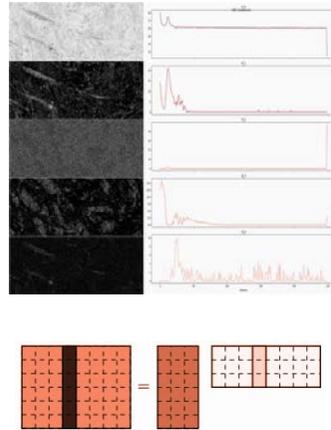


Timeline

Proof of concept

- FFOCT skin cancer detection
- Pixel annotations
- Custom CNN

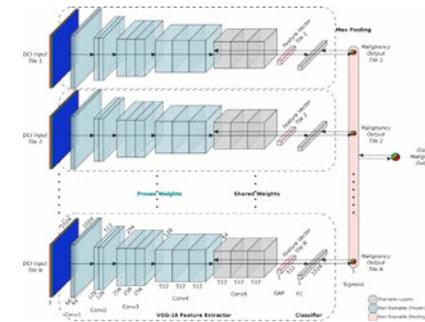
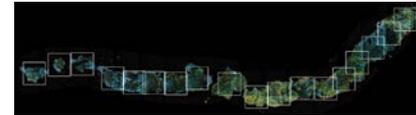
Mandache et al. ISBI 2018



DCI Images

- Fully supervised classification normal vs malignant
- Overcome pathologist performance with 92% and tumor localization with attention

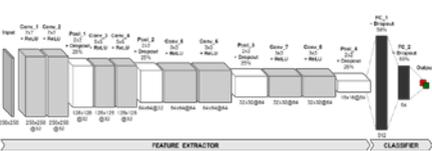
Mandache et al. ISBI 2021



Multimodality

- Cross-modal matching
- Learn common latent space in contrastive learning framework

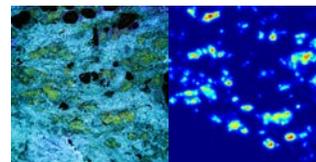
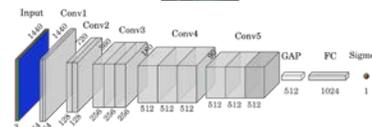
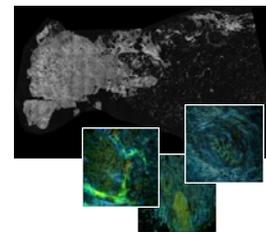
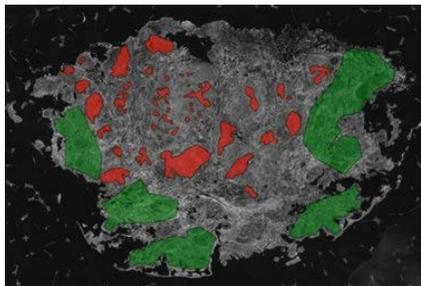
Mandache et al. ISBI 2023



DCI Signal

- Characterize DCI signal, clustering / decomposition on raw signal (unsupervised)
- *paper* : NMF decomposition of DCI signal

Mandache et al. ISBI 2021



Clinical Data

- Annotation scarcity
- Multiple Instance Learning (MIL) based classification benign vs malignant
- *paper* :

Mandache et al. ICIP 2022

